# Laser-hybrid Accelerator for Radiobiological **Applications**

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## INTRODUCTION

LhARA [1] is conceived as a novel, uniquely flexible facility dedicated to the study of the biological response to ionising radiation. With the potential to deliver multiple ion species in beams with a wide range of temporal and spatial profiles at high and ultra-high dose rates. LhARA will enable the exploration of a completely new regime of particle-beam therapy. Funding from the UKRI Infrastructure Fund for a 2-year "Preliminary Activity" to deliver a CDR for the Ion Therapy Research Facility [2] served by LhARA has recently been announced.

- ► A high-power laser will create a large flux of protons or light ions from a foil target.
- Particles are captured and focused using electron plasma lenses.
- ► The fixed-field alternating-gradient accelerator (FFA) provides rapid acceleration and preserves the flexibility of the beam created at the source.



Figure 1: Schematic diagram of the LhARA beam lines. The beam from the source (red arrow) is transported either to the low-energy in vitro end station or the FFA injection line. The accelerated beam is directed either to the high-energy in vitro end station or the in vivo end station.

### LhARA STAGE 1

Stage 1 of LhARA contains all the components from the laser source to the first *in vitro* vertical arc designed for studies with proton beams with energy  $12 \,\mathrm{MeV}$ -15 MeV.



Figure 5: Schematic layout of the Stage 1 beam line. The laser is brought to a focus on the particle-production target. Capture and focusing is provided by a series of Gabor lenses. The final section of the beam line bends the beam vertical and delivers it to the low-energy in vitro end station.

- Preliminary end-to-end tracking of proton beam from laser target to end station.
- ▶ Planned re-optimisation of the magnet strengths for capture and transport.

#### LhARA STAGE 2



## LASER SOURCE

lons are generated via the target normal sheath acceleration (TNSA) mechanism.



Figure 2: Schematic diagram of the laser source (left) and 2D positional spread of protons at 1 ps as simulated with Smilei [3] (middle). Kinetic energy spectrum of the protons produced in the laser-target interaction (right).

An intense laser pulse generates a sheath of electrons at the rear surface of the target. Surfacecontaminant positive ions are accelerated by the strong space-charge field.

- ▶ Ion energies  $>40 \,\mathrm{MeV/u}$  obtained at high laser intensity.
- $\blacktriangleright$  100 TW commercial laser system with a pulse length of 25 fs and repetition rate of 10 Hz is able to deliver a high proton flux (>  $10^9$ ).
- $\blacktriangleright$  Tape drive target is proposed to allow a reproducible proton flux with energy  $\leq 15 \,\mathrm{MeV}$ .
- > Particles captured at energies significantly above those that pertain to conventional facilities, evading the limits on the instantaneous dose rates.
- ▶ Particle production at the source simulated in 2D with particle-in-cell (PIC) code [3].

## **GABOR LENS**

Electron cloud used for compact focussing to capture the large divergence and energy spread of the laser driven ion beam.

- Electron plasma confined within a lens with a configuration of cylindrical electrodes placed in a longitudinal magnetic field.
- Magnetic field greatly reduced compared to a solenoid of the same focal length.
- Lenses and collimator used to select particle



Figure 3: Schematic of a Penning-Malmberg trap

Stage 2 of LhARA consists of the FFA and all downstream elements that are planned to provide proton and ion beams for both in vivo and in vitro studies.



Figure 6: Schematic drawingf of LhARA Stage 2. The Stage 1 beam is injected into tge FFA which delivers proton beam energies between 40 MeV and 127 MeV to in vitro and in vivo end stations. Ion beams with energies up to 34 MeV/nucleon can also be delivered.

▶ Flexible optics configurations to deliver beams between 1 and 30 mm.

# **BIOLOGICAL END STATION**

The *in vitro* end stations are envisaged for the irradiation of 2D monolayer and 3D-cell systems in culture.

- Sealed units allow for cells to be incubated prior to and during irradiation.
- ▶ Robotics will enable cell culture plates to be placed into and taken out of the beam.
- The *in vivo* end stations will be used to irradiate small-animal models.
- ► An image guidance system will be used to enable a high level of precision and accuracy.
- ► The flexibility in beam sizes allows for different irradiation conditions: passive scattering, pencil-beam scanning, and micro-beam irradiation at conventional and FLASH dose rates.

BDSIM was used to evaluate the maximum dose distributions that LhARA can deliver.

▶ The integrated energy deposition within a fixed volume of water at the Bragg peak was recorded:

	Protons			Carbon 6+
	$12\mathrm{MeV}$	$15 \mathrm{MeV}$	<b>127</b> MeV	<b>33.4</b> MeV/u
Dose per pulse	7.1 Gy	12.8 Gy	<b>15.6</b> Gy	<b>73.0</b> Gy
Instantaneous dose rate	$1.0  imes 10^9  { m Gy/s}$	$1.8  imes 10^9  { m Gy/s}$	$3.8  imes 10^8  { m Gy/s}$	$9.7 imes10^8{ m Gy/s}$
Average dose rate	$71\mathrm{Gy/s}$	$128\mathrm{Gy/s}$	$156\mathrm{Gy/s}$	<b>730</b> Gy/s

#### energy.

# proposed for use in the Gabor lens for LhARA

- ► First lens prototype tested at Imperial College and Surrey Ion Beam Centre
- Recent understanding of the plasma instabilities observed with the prototype [4]
- ▶ Theoretical investigation of lens stability is underway with a PIC code [5]

## FIXED-FIELD ALTERNATING-GRADIENT ACCELERATOR (FFA)

A FFA will be used to accelerate the beam in Stage 2 to energies of up to  $127 \,\mathrm{MeV}$  for protons and  $33 \,\mathrm{MeV/u}$  for carbon ions.

- ► Multiple ion capability
- Compact size and low cost
- ► High variable dose delivery
- ► Various of beam energies without the use of a degrader



Figure 4: Layout of the FFA ring.

Table 1: Expected maximum dose rates LhARA can deliver for various beam energies at minimum beam size.

#### CONCLUSION

► LhARA aims to to demonstrate novel technologies and enable a systematic programme of radiobiological studies-both necessary for improving particle therapy.

#### REFERENCES

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