

## Nuclear medicine

### Week 3; Block 6; Section 3: Data acquisition in PET

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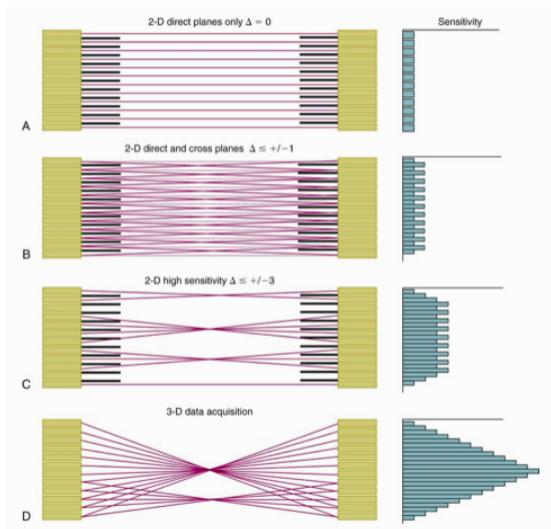
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## Section 3

# Data acquisition in PET

# Event recording topologies



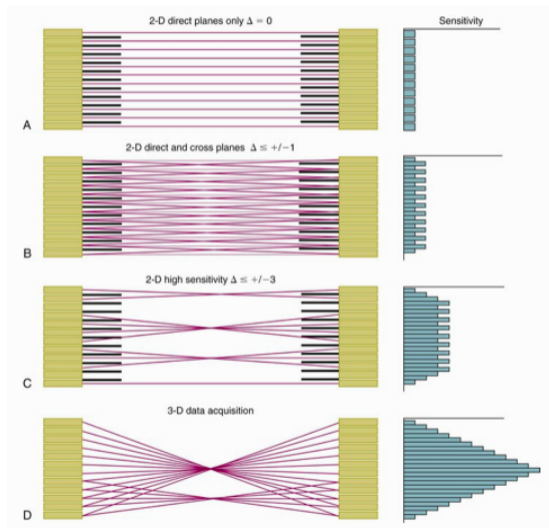
A) 2D data acquisition: septa such that:

- Accept only 'in line'  $\gamma$  pairs
- Reduced rate of scatters & randoms
- Recons: e.g. filtered back projection
- Least efficient

B) Cross planes: septa such that  $\Delta = \pm 1$ :

- Accept coincidences in neighbouring cells
- Increased rate of scatters & randoms
- Scanner centre, effective separation =  $\frac{d}{2}$
- Recons: as in A using effective separation
- For  $n$  rings  $\Rightarrow 2n - 1$  image planes
- Efficiency enhanced

# Event recording topologies



- C) Cross planes: septa such that  $\Delta = \pm 2; \pm 3$ :
- Accept coincs for cells with  $|\Delta| = 1, 2, 3$
  - Increased rate of scatters & randoms
  - Recons: for large  $|\Delta|$  resolution decreases
  - Efficiency enhanced
- D) 3D acquisition mode: no septa
- Accept all coincidences
  - Sensitivity increases  $\times 4 - \times 8$
  - Recons: require 3D algorithm
  - Increased rate of scatters & randoms
  - Most efficient

## Numerical comparison of sensitivities

Histograms in figures A–D indicate spacial dependence of relative efficiency;

→ indicates, for example, object of interest should be in the centre of a 3D scanner

For some 'typical' systems:

- PET scanner in 2D mode (1 slice per detector ring): 0.002–0.005 counts/s/Bq
- PET scanner in 3D mode (coincidences between all rings): 0.02–0.1 counts/s/Bq
- SPECT (for comparison): 0.0001–0.0003 counts/s/Bq

## Summary of section 3

Resolution and sensitivity can be improved by expanding range of allowed coincidences

Sensitivity in PET can exceed that of SPECT by more than a factor of 10