## Magnetic Resonance Imaging

## Week 4; Lecture 8; Section 2: Rotating the magnetisation

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## Section 2

## Rotating the magnetisation

## First, a static example



Consider magnetisation $\mathbf{M}$ parallel to $z$ axis and $\mathbf{B}$ parallel to the $x$ axis, as shown

Torque, $\mathbf{M} \times \mathbf{B}$, is therefore parallel to the $y$ axis

Net result is that $\mathbf{M}$ will precess around the $x$ axis towards the $y$ axis

This is what is done in MRI ...

## Rotating the magnetisation vector in MRI; principle

Main field, $\mathbf{B}_{0}$, produced with solenoid


Induces magnetisation $\mathbf{M}$ parallel to $\mathbf{B}_{0}$

To rotate $\mathbf{M}$ away from $\mathbf{B}_{0}$ require magnetic field in transverse $(x, y)$ plane

Call the field in the $x, y$ plane $\mathbf{B}_{1}$; can be produced with a variety of coil arrangements, e.g. dipole or, more efficient, a "bird cage"


To cause $\mathbf{M}$ to precess require that $\mathbf{M}$ oscillates at the Larmor frequency, $\omega$. I.e. require RF magnetic field $\mathbf{B}_{1}$

## Rotating the magnetisation vector in MRI; mathematics

Take $\mathbf{B}_{1}$ to be "plane polarised" in $x, y$ such that $B_{1_{x}}=B_{1} \cos (\omega t+\alpha)$ and $B_{1_{y}}=B_{1} \sin (\omega t+\beta) ; \alpha$ and $\beta$ are phases
$\mathbf{B}_{1}$ can be rewritten in terms of two circularly polarised fields:


$$
B_{1_{a c}}=\frac{B_{1}}{2} ; \phi_{a c}=\omega t+\alpha^{\prime}
$$



$$
B_{1_{c}}=\frac{B_{1}}{2} ; \phi_{c}=\omega t+\beta^{\prime}
$$

## Rotating the magnetisation vector in MRI

One of the two counter rotating fields will rotate in the same direction as the nuclear precession

In the frame that is co-rotating with the precession of the net magnetisation vector the magnetic field will appear stationary in the transverse $(x, y)$ plane. Call the co-rotating field $B_{1}^{+}$
$B_{1}^{+}$is equal to either $B_{1_{a c}}$ or $B_{1_{c}}$ depending on the direction of $\mathbf{B}_{0}$
The stationary field will therefore cause $\mathbf{M}$ to precess about a rotating axis in the $(x, y)$ plane
The net result is that $\mathbf{M}$ can be rotated into the $x, y$ plane where it will continue to precess
The precession of $\mathbf{M}$ in the $x, y$ plane gives a detectable RF signal

## Rotating the magnetisation vector in MRI

$\mathbf{M}$ is initially parallel to $\mathrm{B}_{0}$

(a) Laboratory Frame of Reference

(b) Rotating Frame of Reference

## The flip angle

The flip angle, $\alpha$, is proportional to the magnitude and duration of the RF pulse:

$$
\alpha=\neq B_{1} t_{P}
$$

where $t_{P}$ is the duration of the RF pulse
$90^{\circ}$ pulse rotates magnetisation into transverse plane where it continues to precess
Effect of $90^{\circ}$ RF Pulse



Example: calculating the duration of a $90^{\circ}$ pulse

RF transverse magnetic field pulse is applied to rotate $\mathbf{M}$

The magnitude of $B_{1}$ is $10 \mu \mathrm{~T}$ (i.e. $10^{-5} \mathrm{~T}$ )

At what rate with the $\mathbf{M}$ rotate away from the $\mathbf{B}_{0}$ axis?

How long will it take for the flip angle to reach $90^{\circ}$ ?

## Example: calculating the duration of a $90^{\circ}$ pulse

Half an answer ...

The magnitude of $B_{1}$ is $10 \mu \mathrm{~T}$ (i.e. $10^{-5} \mathrm{~T}$ )

At what rate with the $\mathbf{M}$ rotate away from the $\mathbf{B}_{0}$ axis?
It will rotate at the Larmor frequency, $f_{1}$ arising from the field $B_{1}$, i.e. $f_{1}=\neq B_{1}$

How long will it take for the flip angle to reach $90^{\circ}$ ?
The angle can be obtained by solving the equation:

$$
\begin{gathered}
\frac{1}{4}=\psi B_{1} t_{P}^{90^{\circ}} \text { for } t_{P}^{90^{\circ}} \\
\text { or } \frac{\pi}{2}=\gamma B_{1} t_{P}^{90^{\circ}}
\end{gathered}
$$

## Summary of section 2

Net magnetisation of ${ }^{1} \mathrm{H}$ spins caused to rotate using plane-polarised, time-varying magnetic field in the $x, y$ plane

Precession of rotated net-magnetisation vector gives rise to RF signal which can be detected

Measurement of the RF signal from the precession of rotated net-magnetisation vector is the basis of MRI

